

This is the accepted manuscript (postprint) of the following article:

E. Salahinejad, M.J. Hadianfard, M. Ghaffari, S. Bagheri Mashhadi, A.K. Okyay, *Fabrication of nanostructured medical-grade stainless steel by mechanical alloying and subsequent liquid-phase sintering*, Metallurgical and Materials Transactions A, 43 (2012) 2994-2998.
<https://doi.org/10.1007/s11661-012-1186-5>

Fabrication of nanostructured medical-grade stainless steel by mechanical alloying and subsequent liquid-phase sintering

E. Salahinejad ^{a,*}, M.J. Hadianfard ^a, M. Ghaffari ^{b,c}, Sh. Bagheri Mashhadi ^a, A.K. Okyay ^b

^a Department of Materials Science and Engineering, School of Engineering, Shiraz University, Zand Blvd., 7134851154, Shiraz, Iran

^b Department of Electrical and Electronics Engineering, UNAM - National Institute of Materials Science and Nanotechnology, Bilkent University,
Ankara 06800, Turkey

^c School of Electrical and Electronic Engineering, Micro Electronic Division, Nanyang Technological University, Nanyang Avenue, Singapore
639798, Singapore

Abstract

This paper focuses on the microstructure of medical-grade P558 (ASTM F2581) stainless steel produced by mechanical alloying and liquid-phase sintering. Rietveld X-ray diffraction and transmission electron microscopy reflect that the mechanically alloyed stainless steel powder is a nanocrystal dispersed amorphous matrix composite. Mn-11.5 wt.% Si eutectic alloy as additive improves densification of the synthesized P558 alloy via liquid-phase sintering mechanism. X-ray mapping shows that after sintering at 1050 °C for 1 h, a uniform distribution of dissolved Mn and Si is achieved. Moreover, the development of a nanostructured fully-austenitic stainless steel after sintering at the same temperature is realized by X-ray diffraction and transmission electron microscopy.

* **Corresponding Author:** Email address: <erfan.salahinejad@gmail.com> (E. Salahinejad)

This is the accepted manuscript (postprint) of the following article:

E. Salahinejad, M.J. Hadianfard, M. Ghaffari, S. Bagheri Mashhadi, A.K. Okyay, *Fabrication of nanostructured medical-grade stainless steel by mechanical alloying and subsequent liquid-phase sintering*, *Metallurgical and Materials Transactions A*, 43 (2012) 2994-2998.
<https://doi.org/10.1007/s11661-012-1186-5>

Keywords: Microstructure; Nano materials; Medical-grade stainless steel; Liquid-phase sintering

1. Introduction

To meet the best mechanical and corrosion behaviors of powder metallurgy parts, it is well established that high densities are imperative. To do so, a number of approaches like warm compaction, increasing sintering temperature and time, and using proper additives to activate liquid-phase sintering are consideration. In the liquid-phase sintering process, the formation of a liquid phase promotes densification via providing a particle rearrangement, faster diffusion rate, and pore elimination [1,2], opening up the further commercial development of powder metallurgy parts. Concerning powder metallurgy of stainless steels, since high solid-state sintering temperatures generally more than 1300 °C are required to obtain a high density [3,4], their liquid-phase sintering process lowering sintering temperature and time is a promising field from scientific and technological viewpoints. To activate liquid-phase sintering of these alloys, various additives like Cu, Sn, Ni, Pt, Ag, Si, Au, B, P, their compounds and alloys have been investigated [1,2].

Austenitic stainless steels, typically AISI 316L, are conventionally used in medical applications; nevertheless, the harmful effects of nickel ions released from this type of implants have provided a high level of motivation for the further development of nickel-free alloys [5]. In the ASTM standards, two nickel-free medical grade stainless steels have been imported: ASTM F2229 (nominated as Biodur 108) and ASTM F2581 (nominated as P558). In the recent years, in vitro and in vivo studies have been conducted on the latter having the

This is the accepted manuscript (postprint) of the following article:

E. Salahinejad, M.J. Hadianfard, M. Ghaffari, S. Bagheri Mashhadi, A.K. Okyay, *Fabrication of nanostructured medical-grade stainless steel by mechanical alloying and subsequent liquid-phase sintering*, Metallurgical and Materials Transactions A, 43 (2012) 2994-2998.
<https://doi.org/10.1007/s11661-012-1186-5>

nominal composition of Fe–17Cr–10Mn–3Mo–0.4Si–0.5N–0.2C from the viewpoints of biocompatibility, osseointegration, and corrosion behaviors [6-11].

It is well established that mechanical alloying (MA) can develop a wide variety of equilibrium and non-equilibrium structures including nanostructured and amorphous powders [12]. In this work, mechanically alloyed P558 stainless steel powder is liquid-phase sintered with a biocompatible sintering aid (Mn–11.5 wt.% Si) and then the resultant microstructure is evaluated via X-ray diffraction, scanning electron microscopy, X-ray mapping, and transmission electron microscopy.

2. Experimental work

P558 (ASTM F2581, Fe–17Cr–10Mn–3Mo–0.4Si–0.5N–0.2C in wt.%) and Mn–11.5 wt.% Si alloy powders were separately processed by MA of Fe, Cr, Mn, Mo, Si, and C (Merck) and iron nitride (Alfa Aesar) powders. Milling was performed in a planetary ball mill with a ball-to-powder weight ratio of 20:1 at a rotation speed of 500 rpm for 48 h under an argon atmosphere. Four bearing steel balls of 20-mm and twelve bearing steel balls of 8-mm diameters with a composition of Fe–1.5Cr–0.9C–0.8Si–0.5Mn were used in this work.

The microstructure of the stainless steel powder was studied by X-ray diffraction (XRD, Shimadzu Lab X-6000 with Cu K α radiation) with a step size of 0.03 and a step time of 4 s. The XRD data were analyzed by MAUD program [13] employing the Rietveld refinement to estimate the phase contents and the crystallite sizes by the Double-Voigt approach. In addition, the synthesized powder particles were dispersed in ethanol, dropped down to a copper grid, and characterized by a transmission electron microscope (TEM, FEI–Tecnai G2F30).

This is the accepted manuscript (postprint) of the following article:

E. Salahinejad, M.J. Hadianfard, M. Ghaffari, S. Bagheri Mashhadi, A.K. Okyay, *Fabrication of nanostructured medical-grade stainless steel by mechanical alloying and subsequent liquid-phase sintering*, Metallurgical and Materials Transactions A, 43 (2012) 2994-2998.
<https://doi.org/10.1007/s11661-012-1186-5>

The milled stainless steel powder was mixed with 6 wt.% additive powder, milled in acetone for 1 h, and dried at 70 °C, encapsulated in evacuated quartz tubes, annealed at 900 °C for 15 min, and finally quenched in water. The obtained powders were pressed using a single acting press at a pressure of 1 GPa without any lubrication. The densification process was followed by sintering at 1000, 1050, 1100, 1150, and 1200 °C for 1 h in evacuated quartz tubes and then water-quenching. Sintered densities were determined by the Archimedes water immersion method. The distribution of the additive elements in the structure was analyzed via X-ray mapping (XMAP) by a scanning electron microscope (SEM, FEI-Quanta 200 FEG). Moreover, the resultant microstructure after sintering was studied by XRD and TEM. For the TEM sample preparation, a selected sintered specimen was cut into a disc of 3 mm in diameter, ground to about 100 μm in thickness, and then electropolished.

3. Results and discussion

The XRD pattern and TEM micrograph of the as-milled P558 powder are shown in Fig. 1. Based on the Rietveld XRD quantitative analysis (the procedure has been detailed in Ref. [14]), this powder consists of 10 % ferrite (α), 48 % austenite (γ) and 42 % an amorphous phase, where the crystallite size of the ferrite and austenite phases is 11.5 and 12 nm respectively, measured by the Double-Voigt approach. Note that the relatively low signal-to-noise ratio in the XRD pattern is due to the presence of the amorphous phase in the material. The selected area diffraction pattern of the TEM micrograph in Fig. 1b includes some diffraction spots related to the crystalline phases and a halo pattern related to the amorphous phase, confirming that the material has an amorphous/nanocrystalline structure. It is noteworthy that in bright-field TEM images those crystallites which are close to a zone-axis

This is the accepted manuscript (postprint) of the following article:

E. Salahinejad, M.J. Hadianfard, M. Ghaffari, S. Bagheri Mashhadi, A.K. Okyay, *Fabrication of nanostructured medical-grade stainless steel by mechanical alloying and subsequent liquid-phase sintering*, Metallurgical and Materials Transactions A, 43 (2012) 2994-2998.

<https://doi.org/10.1007/s11661-012-1186-5>

orientation appear dark; in contrast, all crystallites which are far off a zone-axis orientation appear bright like the amorphous phase. Additionally, Fig. 1c presents the high-resolution TEM micrograph of the same powder, in which a consideration to the atomic arrangement depicts a crystalline region embedded in the amorphous matrix, inferring the heterogeneous nucleation of the amorphous phase from grain boundaries of the crystalline phases as high-energy places which are preferential for nucleation [15,16]. The significant structural refinement leading to nanocrystallization can be explained by severe plastic deformation (due to the actions of the milling media [12]) and the contribution of the interstitially dissolved elements (C and N). Nitrogen [14,17] and carbon [18] atoms are segregated at dislocations and grain boundaries, fixing the dislocations and stabilizing the grain boundaries. Consequently, the trickling down of mobile dislocations on the fixed dislocations contributes to the nucleation of new boundaries and a severe grain refinement. A similar contribution to structural refinement has been attributed to the interstitial dissolution of boron in mechanically alloyed Co-based powders [19]. Moreover, amorphization can be explained by severe plastic deformation (accordingly extreme structural refinement), large atomic size mismatch and negative enthalpy of mixing among the constituent elements [14,15,17,19].

Fig. 2 indicates the sintered densities measured by the Archimedes water immersion method. It can be seen that by increasing the sintering temperature and adding the sintering aid, higher densities are achieved. For the samples containing the sintering aid, a sharp increase in density occurs when the sintering temperature increases from 1000 °C to 1050 °C, followed by a lower rate densification with the further temperature increase. The additive (Mn–11.5 wt.% Si) is a eutectic alloy with a eutectic temperature of 1040 °C [20]. The formation of the eutectic liquid phase at the temperatures higher than 1040 °C activates the

This is the accepted manuscript (postprint) of the following article:

E. Salahinejad, M.J. Hadianfard, M. Ghaffari, S. Bagheri Mashhadi, A.K. Okyay, *Fabrication of nanostructured medical-grade stainless steel by mechanical alloying and subsequent liquid-phase sintering*, Metallurgical and Materials Transactions A, 43 (2012) 2994-2998.
<https://doi.org/10.1007/s11661-012-1186-5>

liquid phase sintering process. Indeed, the formed liquid at the additive particle sites wets the main powder particles, penetrates the particle contacts and pore zones via capillary forces, and provides a path of high diffusivity. With increasing the sintering temperature beyond 1050 °C, the decrease in the formed liquid viscosity, the increase in wetting characteristics, the increase in diffusivity, and possibly the increase in the liquid phase amount are responsible for densification [1,2].

Fig. 3a presents the SEM micrograph of the sample containing 6 % additive sintered at 1050 °C for 1 h. Small, relatively spherical, and isolated pores observed, despite the practiced sintering temperature which is low for solid-state sintering, implies activation of the liquid phase sintering mechanism. Manganese and Silicon XMAP (Figs. 3b and 3c) confirms the complete dissolution, no evidence of precipitation, and the uniform distribution of the additive elements in the structure in a scale comparable with the stainless steel particle size (SEM observations of the P558 powder suggested that the particles are almost 20 μm in size). In addition, the uniform distribution of Cr in the structure (Fig. 3d), which is critical for corrosion protection, infers the merit of processing. The achievement of this uniform microstructure is explained by liquation of the Mn–Si eutectic additive and thereby providing a path of high diffusivity. On the other hand, considering the mean size of the main powder particles which is almost 20 μm, the mean diffusion length is estimated to be 10 μm. Indeed, this short diffusion length and the high-diffusivity liquid path justify the development of this homogeneous structure by sintering at 1050 °C for 60 min.

The XRD pattern and TEM micrograph of the additive-containing sample sintered at 1050 °C are provided in Fig. 4. Analyzing the XRD pattern by MAUD software reflects that the material is fully austenitic based on Rietveld analyses considering all probable phases like

This is the accepted manuscript (postprint) of the following article:

E. Salahinejad, M.J. Hadianfard, M. Ghaffari, S. Bagheri Mashhadi, A.K. Okyay, *Fabrication of nanostructured medical-grade stainless steel by mechanical alloying and subsequent liquid-phase sintering*, *Metallurgical and Materials Transactions A*, 43 (2012) 2994-2998.
<https://doi.org/10.1007/s11661-012-1186-5>

nitrides, carbides, and ferrites, demonstrating the competence of the austenitization thermal cycle applied. Albeit, it should be considered that very low phase contents cannot be detected by XRD. According to the TEM micrograph depicted in Fig. 4b, the austenite grain size is almost 25 nm. Considering the atomic arrangement in the high-resolution TEM micrograph (Fig. 4c), crystallinity of each unit in Fig. 4b (as a crystalline grain) is confirmed. It is also noticeable that the crystallite size measured by XRD is 35 nm, although it is expected that the XRD crystallite size is smaller than the TEM grain size. It may be due to the fact that the TEM observation is local, but XRD considers more crystallites. The development of these nanostructures despite the sintering process reflects a considerable thermal stability and an inherent resistance to grain growth, which is in accordance with findings for other multicomponent nanostructures [21,22]. Typically, Cisneros et al. [21] reported austenite grain sizes smaller than 70 nm for mechanically alloyed Fe–18Cr–11Mn–(0.27-2.47)N stainless steel nanostructures after annealing at 900, 1000, 1100, and 1200 °C for 2 h. It is known that grain growth is strongly controlled by grain boundary diffusion and mobility. The factors affecting grain boundary mobility in nanostructured materials include grain boundary segregation, solute impurity, porosity, chemical ordering, and second phases [21]. Indeed, in this study, solute drag effects combined with the typical contribution of carbon and nitrogen are expected to retard grain growth. The solubility of the interstitially dissolved atoms of nitrogen and carbon in the crystalline phases is limited; thus, they tend to segregate at grain boundaries to decrease strain energy, thereby retarding grain boundary mobility. Furthermore, slow crystallization of the amorphous phase developed during MA as a diffusional phase transformation demanding time can affect the final grain size [23].

This is the accepted manuscript (postprint) of the following article:

E. Salahinejad, M.J. Hadianfard, M. Ghaffari, S. Bagheri Mashhadi, A.K. Okyay, *Fabrication of nanostructured medical-grade stainless steel by mechanical alloying and subsequent liquid-phase sintering*, Metallurgical and Materials Transactions A, 43 (2012) 2994-2998.

<https://doi.org/10.1007/s11661-012-1186-5>

It is also noteworthy that the final chemical composition of the additive-containing sample would be Fe–16Cr–14.7Mn–2.8Mo–1Si–0.47N–0.19C. This composition variation as a result of the sintering aid addition, i.e. the increase in the Mn and Si content and the decrease in the other elements' amount, could affect mechanical and electrochemical properties. On the other hand, the positive effect of the additive on the increase of density and the decrease of pores should be considered, which demands comprehensive studies on their mechanical and corrosion properties.

4. Conclusions

The microstructure of a medical-grade stainless steel produced by mechanical alloying and subsequent liquid-phase sintering processes was investigated. The following results emerge from the present study:

- MA of the stainless steel powder for 48 h processed a nanocrystal dispersed amorphous matrix composite.
- Mn-Si eutectic alloy as additive successfully activated the liquid-phase sintering mechanism in the P558 alloy powder.
- A uniform distribution of Mn, Si, and Cr was realized in the material sintered at 1050 °C.
- Sintering at 1050 °C for 1 h developed a fully-austenitic nanostructure with grains of 25 nm in size.

References

[1] R.M. German: Powder Metallurgy Science, 2nd ed., Metal Powder Industry Federation, 1994, pp. 99-109.

This is the accepted manuscript (postprint) of the following article:

E. Salahinejad, M.J. Hadianfard, M. Ghaffari, S. Bagheri Mashhadi, A.K. Okyay, *Fabrication of nanostructured medical-grade stainless steel by mechanical alloying and subsequent liquid-phase sintering*, Metallurgical and Materials Transactions A, 43 (2012) 2994-2998.

<https://doi.org/10.1007/s11661-012-1186-5>

- [2] E. Klar and P.K. Samal: Powder Metallurgy Stainless Steels: Processing, Microstructures, and Properties, ASM International, 2007, pp. 59-100.
- [3] J.A.C. Miramontes, J.D.O.B. Sanchez, F.A. Calderon, A.M.. Villafane and J.G.C. Nava: J. Mater. Eng. Perform. 2010, vol. 19, pp. 880-4.
- [4] M Youseffi and K.Y. Chong: Powder Metall. 2003, vol. 46, pp. 30-8.
- [5] K. Yang and Y. Ren: Sci. Technol. Adv. Mater. 2010, vol. 11, pp. 1-13.
- [6] U.I. Thomann, P.J. Uggowitzer, Wear 239 (2000) 48-58.
- [7] M. Fini, A.N. Nicoli, P. Torricelli, G. Giavaresi, V. Borsari, H. Lenger, J. Bernauer, R. Giardino, R. Chiesa, A. Cigada, Biomaterials 24 (2003) 4929-4939.
- [8] L. Montanaro, M. Cervellati, D. Campoccia, C. Renata Arciola, J. Mater. Sci.: Mater. Med. 17 (2006) 267-275.
- [9] Y. Ren, H. Yang, K. Yang, B. Zhang, Key Eng. Mater. 342-343 (2007) 605-608.
- [10] R.F.V.V. Jaimes, M.L.C.A. Afonso, S.O. Rogero, S.M.L. Agostinho, C.A. Barbosa, Mater. Lett. 64 (2010) 1476-1479.
- [11] J. Buhagiar, L. Qian, H. Dong, Surf. Coat. Technol. 205 (2010) 388-395.
- [12] C. Suryanarayana: Prog. Mater. Sci., 2001, vol. 46, pp. 1-184.
- [13] L. Lutterotti: MAUD CPD Newsletter (IUCr), 2000, no. 24.
- [14] R. Amini, M.J. Hadianfard, E. Salahinejad, M. Marasi and T. Sritharan: J. Mater. Sci., 2009, vol. 44, pp. 136-48.
- [15] M. Mendez, H. Mancha, M.M. Cisneros, G. Mendoza, J.I. Escalante and H.F. Lopez: Metall. Mater. Trans. A, 2002, vol. 33A, pp. 3273-8.
- [16] E. Ma and M. Atzomon: Mater. Chem. Phys., 1995, vol. 39, pp. 249-67.

This is the accepted manuscript (postprint) of the following article:

E. Salahinejad, M.J. Hadianfard, M. Ghaffari, S. Bagheri Mashhadi, A.K. Okyay, *Fabrication of nanostructured medical-grade stainless steel by mechanical alloying and subsequent liquid-phase sintering*, Metallurgical and Materials Transactions A, 43 (2012) 2994-2998.

<https://doi.org/10.1007/s11661-012-1186-5>

- [17] E. Salahinejad, R. Amini and M.J. Hadianfard: Powder Technol. 2012, vol. 215-216, pp. 247-53.
- [18] E.P. Yelsukov, G.A. Dorofeev, A.V. Zagainov, N.F. Vildanova and A.N. Maratkanova: Mater. Sci. Eng. A, 2004, vol. 369, pp. 16-22.
- [19] A.H. Taghvaei, M. Stoica, G. Vaughan, M. Ghaffari, S. Maleksaeedi and K. Janghorban: J. Alloys Compd., 2012, vol. 512, pp. 85-93.
- [20] ASM Handbook: Alloy Phase Diagrams, ASM International, vol. 3, 2003.
- [21] M.M. Cisneros, H.F. Lopez, H. Mancha, D. Vazquez, E. Valdes, G. Mendoza and M. Mendez: Metall. Mater. Trans. A, 2002, vol. 33A, pp. 2139-44
- [22] K. Lu, Z.F. Dong, I. Bakonyi and A. Cziraki: Acta Metall. Mater., 1995, vol. 43, pp. 2641-7.
- [23] R. Amini, E. Salahinejad, E. Askari Bajestani and M.J. Hadianfard: J. Alloys Compd. 2011, vol. 509, pp. 3252-6.

This is the accepted manuscript (postprint) of the following article:

E. Salahinejad, M.J. Hadianfard, M. Ghaffari, S. Bagheri Mashhadi, A.K. Okyay, *Fabrication of nanostructured medical-grade stainless steel by mechanical alloying and subsequent liquid-phase sintering*, Metallurgical and Materials Transactions A, 43 (2012) 2994-2998.
<https://doi.org/10.1007/s11661-012-1186-5>

Figures

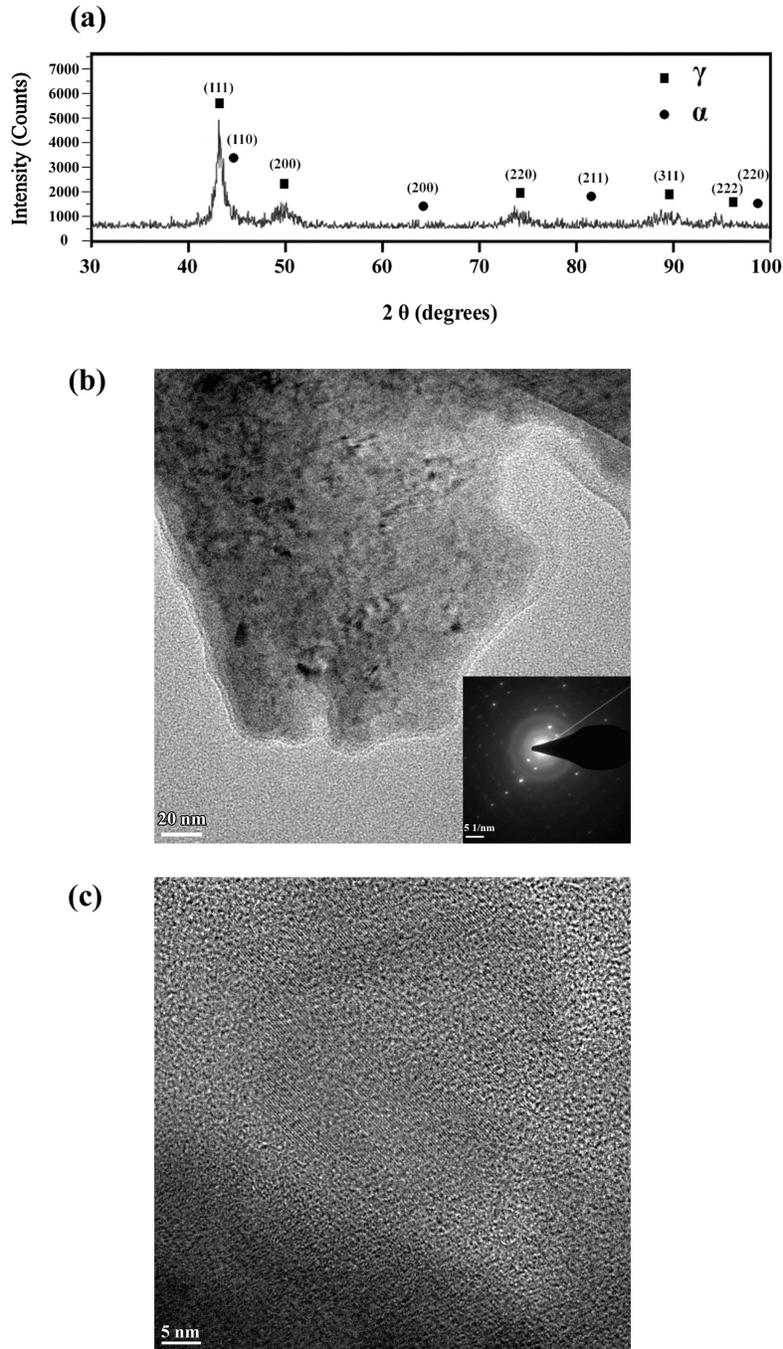


Fig. 1. XRD pattern (a) TEM micrograph (b), and high-resolution TEM micrograph (c) of the as-milled P558 powder.

This is the accepted manuscript (postprint) of the following article:

E. Salahinejad, M.J. Hadianfard, M. Ghaffari, S. Bagheri Mashhadi, A.K. Okyay, *Fabrication of nanostructured medical-grade stainless steel by mechanical alloying and subsequent liquid-phase sintering*, Metallurgical and Materials Transactions A, 43 (2012) 2994-2998.
<https://doi.org/10.1007/s11661-012-1186-5>

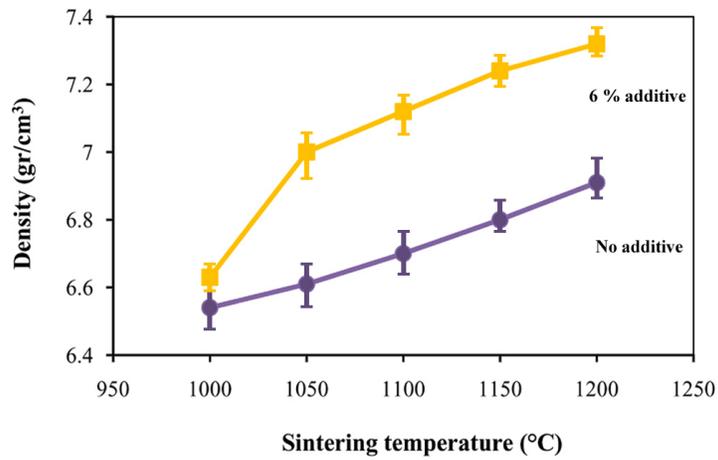


Fig. 2. Sintered densities measured by the Archimedes water immersion method.

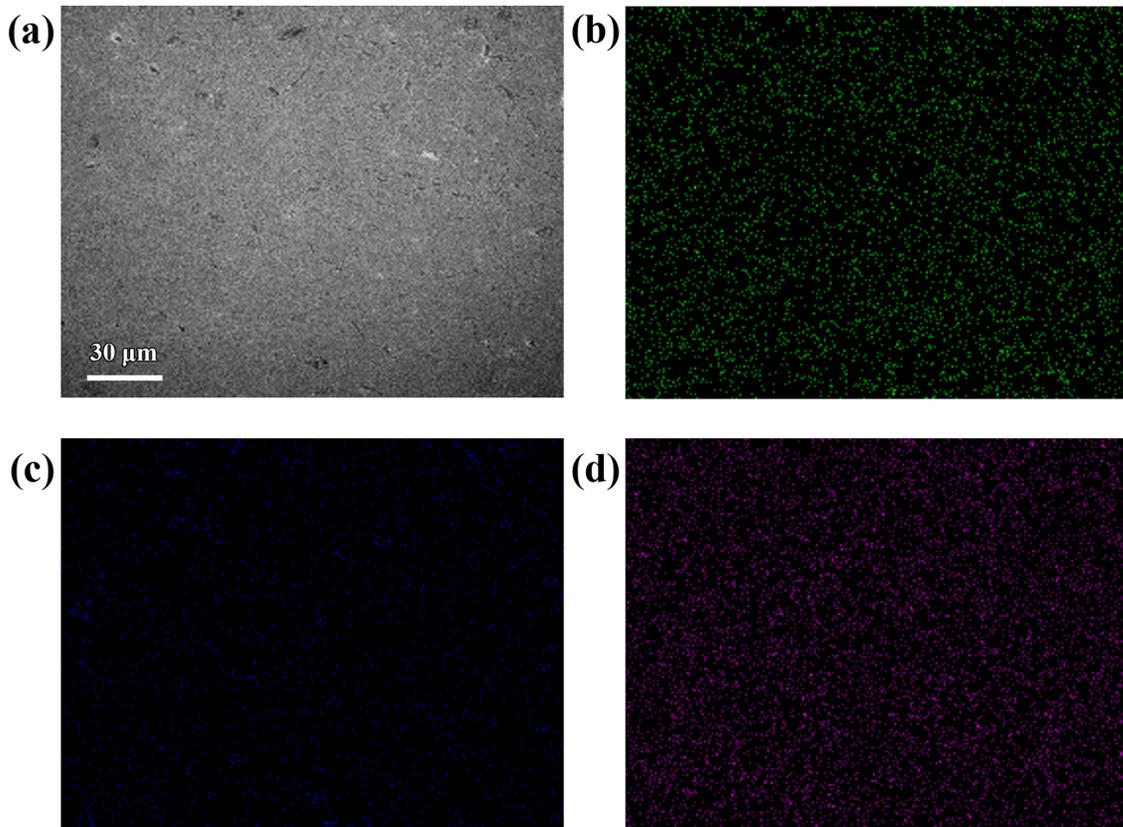


Fig. 3. SEM micrograph (a) and XMAP of Mn (b), Si (c), and Cr (d) for the additive-containing sample sintered at 1050 °C.

This is the accepted manuscript (postprint) of the following article:

E. Salahinejad, M.J. Hadianfard, M. Ghaffari, S. Bagheri Mashhadi, A.K. Okyay, *Fabrication of nanostructured medical-grade stainless steel by mechanical alloying and subsequent liquid-phase sintering*, *Metallurgical and Materials Transactions A*, 43 (2012) 2994-2998.

<https://doi.org/10.1007/s11661-012-1186-5>

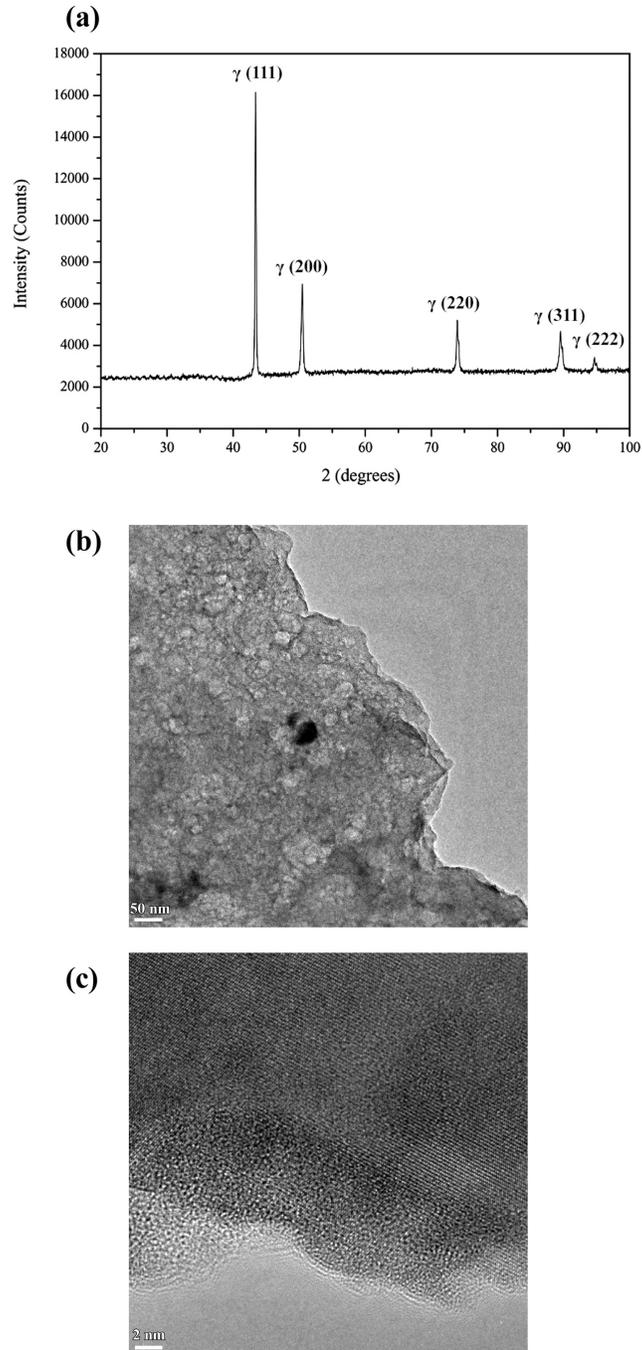


Fig. 4. XRD pattern (a), TEM micrograph (b), and high-resolution TEM micrograph (c) of the additive-containing sample sintered at 1050 °C.